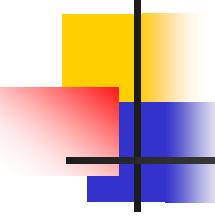


Data processing and refinement

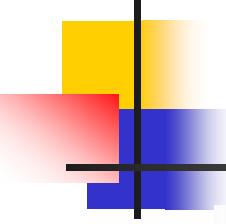


P. Schapotschnikow

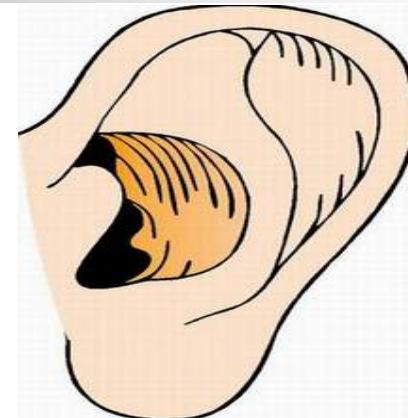


Contents

1. Introduction
2. Tomography reconstruction problem
3. Fourier Transform
4. Data refinement

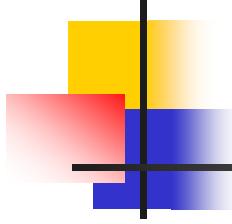


Vision vs Hearing



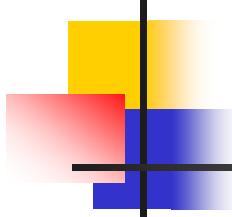
- High 2D resolution
- 3D reconstruction
- Different receptors allow colour vision

- Low spatial resolution
- Reconstruction of different sounds in a mixture



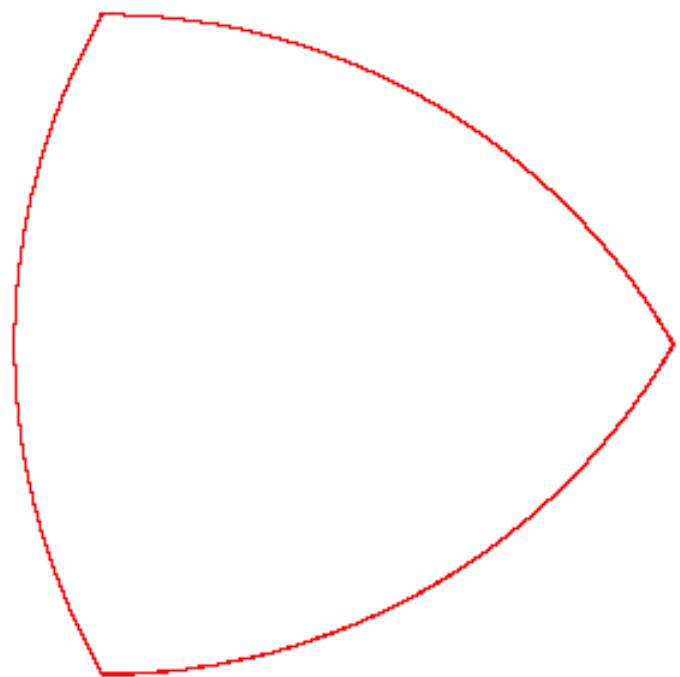
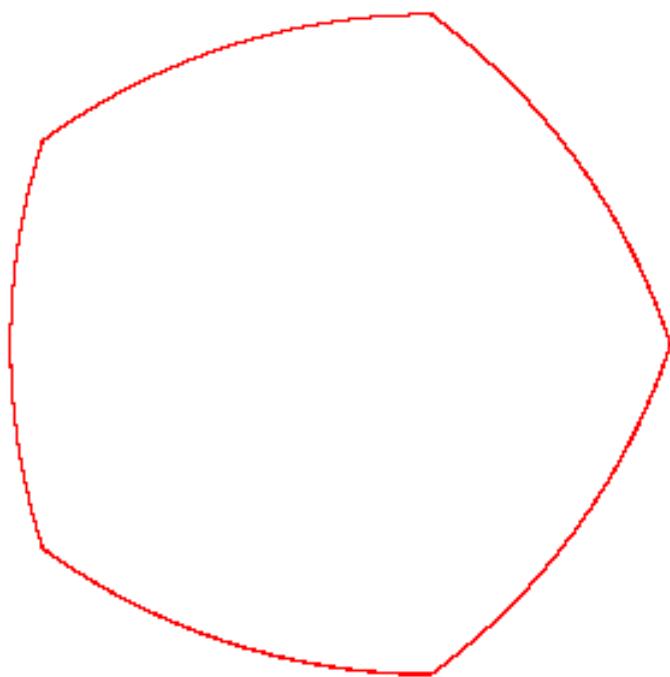
2D reconstruction from silhouettes

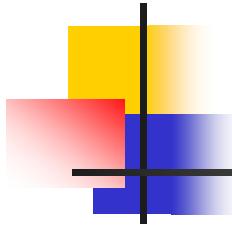
Is it possible to reconstruct a convex object given all 2D parallel-beam silhouettes?



2D reconstruction from silhouettes

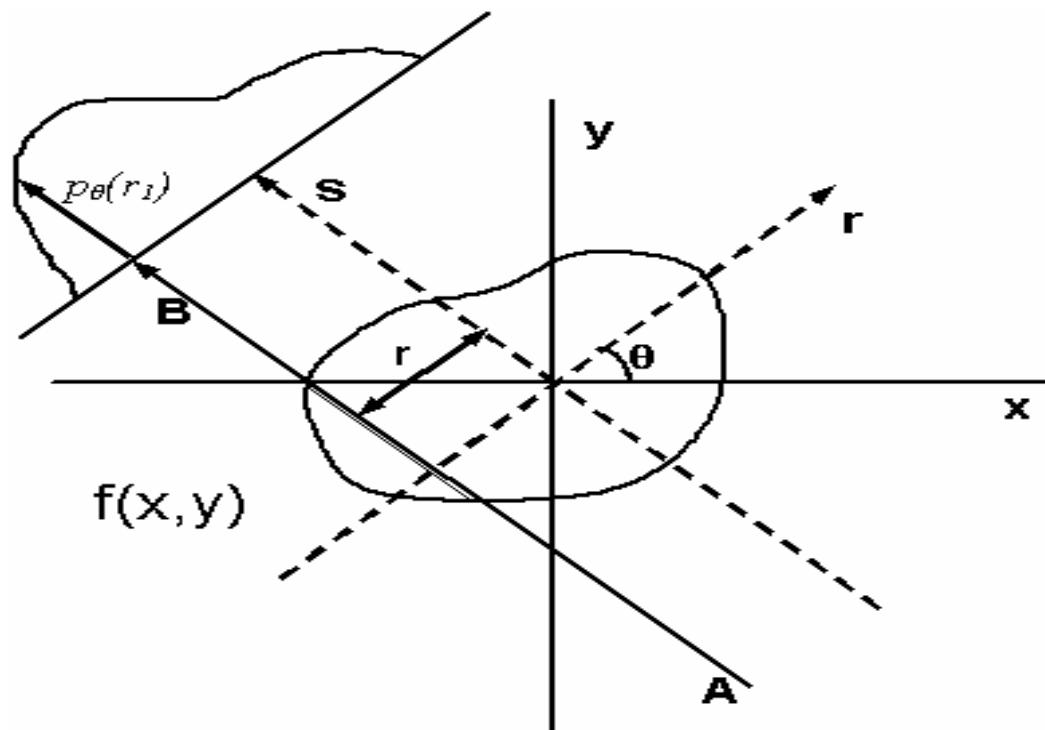
NOT UNIQUELY!!

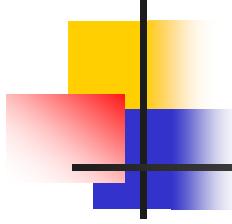




Tomography reconstruction

CT: reconstruction from X-Ray shadows



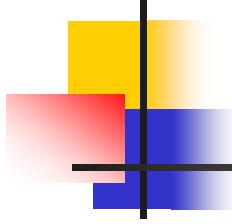


Tomography reconstruction

- Intensity of shadows: Beer-Lambert law

$$I = I_0 \exp(-\int \mu(x)dx)$$

- $\mu(x)$ is the attenuation coefficient varying for different tissues
- Silhouettes are special cases with infinite attenuation



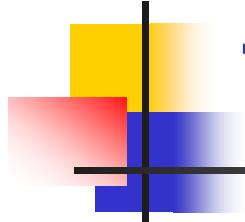
Tomography reconstruction

- Radon transform

$$\ln \frac{I_0}{I} = \int_{l(r,\theta)} \mu(\vec{x}) dx = p(r, \theta)$$

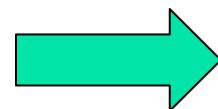
- Inverse Radon transform

$$\mu(\vec{x}) = \frac{1}{2\pi^2} \int_0^\pi \int_{-\infty}^{\infty} \frac{1}{x_1 \cos \theta + x_2 \sin \theta - r} \frac{\partial p(r, \theta)}{\partial r} dr d\theta$$

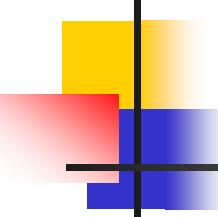


Tomography reconstruction

- Problem: the iRT is discontinuous!

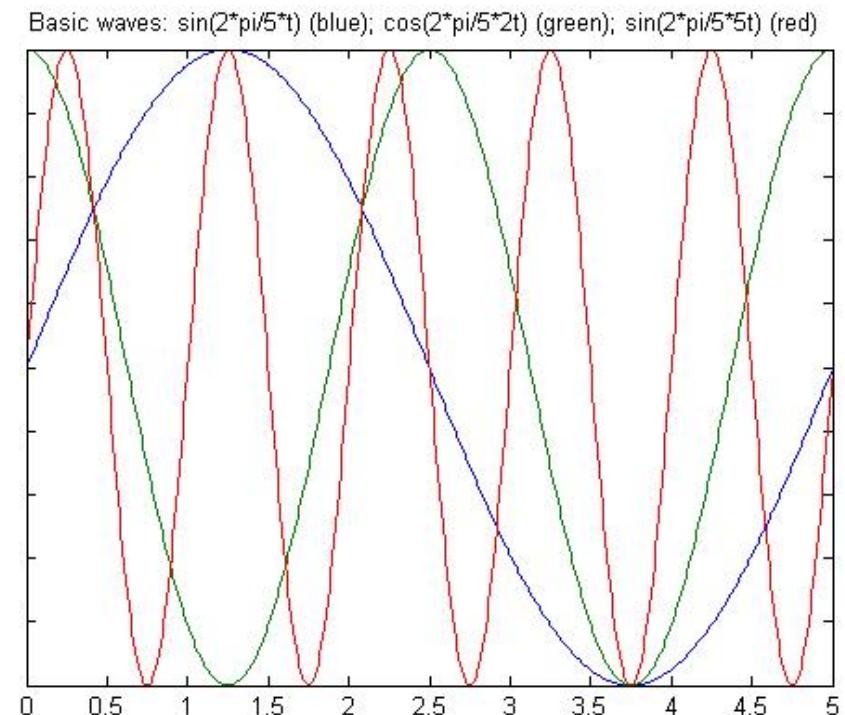
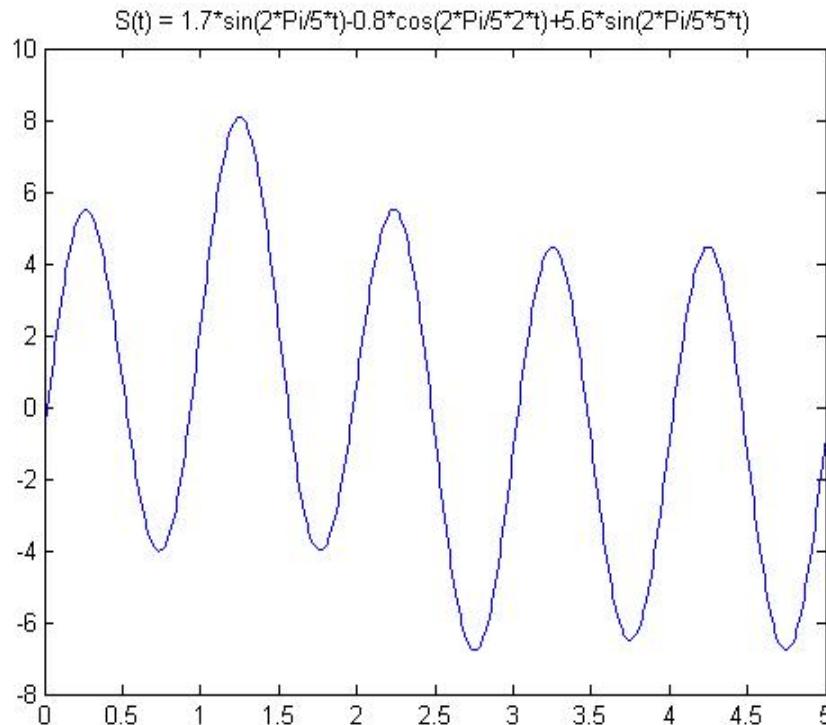


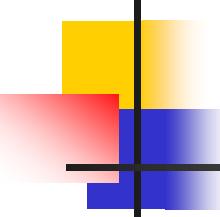
Filtered Back-Projection



Fourier Transform

- Task: find the share of a basic signal in a mixture





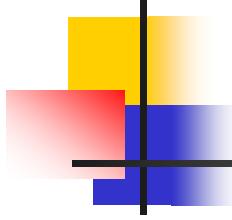
Fourier Transform

- Trick: integrate with the required mode

$$\int_0^T S(t) \sin\left(\frac{2\pi}{T}t\right) dt =$$

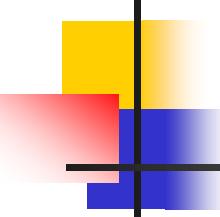
$$\int_0^T b_1 \sin^2\left(\frac{2\pi}{T}t\right) dt + \int_0^T a_2 \sin\left(\frac{2\pi}{T}t\right) \cos\left(\frac{2\pi}{T}2x\right) dt + \int_0^T b_5 \sin\left(\frac{2\pi}{T}t\right) \sin\left(\frac{2\pi}{T}5x\right) dt =$$

$$\frac{T}{2}b_1 + 0 + 0.$$



Fourier Transform

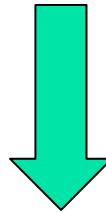
- Every signal can be split in frequencies k/T
- Frequency resolution is determined by the time range



Fourier Transform

- Complexification: deMoivre formula

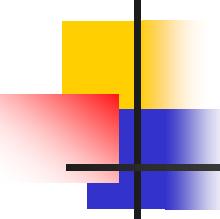
$$\exp(ix) = \cos(x) + i \sin(x)$$



$$a \cos(\omega x) + b \sin(\omega x) = c_+ \exp(i\omega x) + c_- \exp(-i\omega x)$$

$$a = c_+ + c_-$$

$$b = i(c_+ - c_-).$$



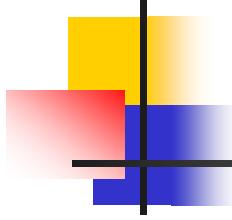
Fourier Transform

- Discretise the time domain:

$$T \longrightarrow N\Delta t$$



$$\text{Integral } dt \longrightarrow \text{sum } \Delta t$$



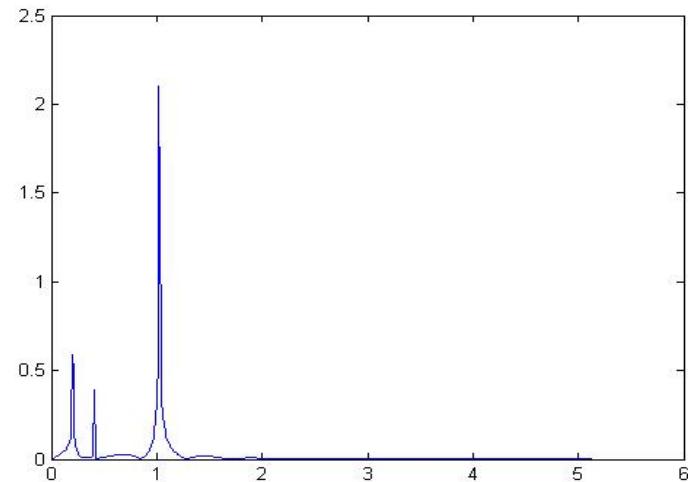
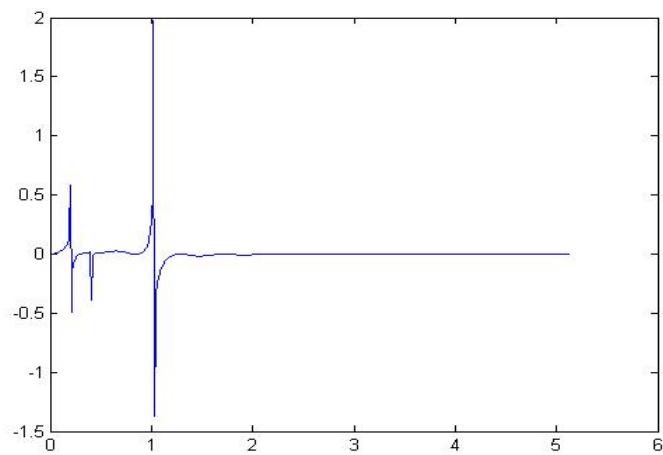
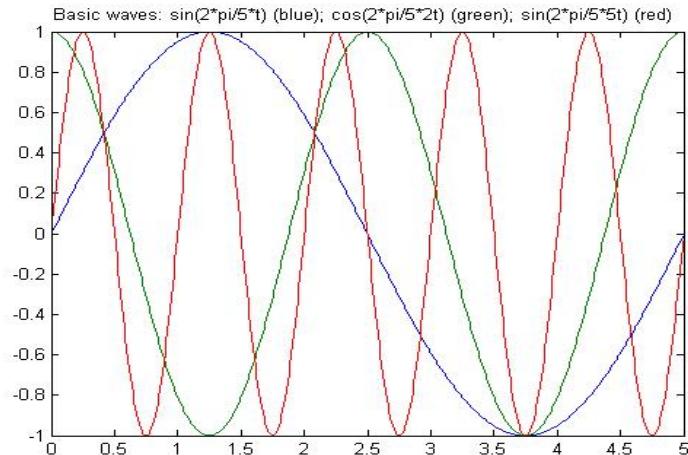
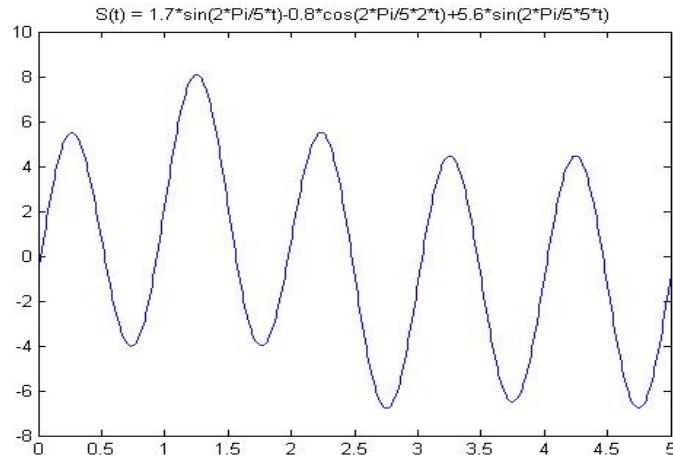
Fourier Transform

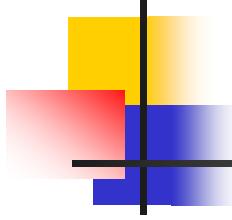
- Discrete Fourier Transform

$$c_k = \frac{1}{N} \sum_{n=0}^{N-1} \exp(-i2\pi kn / N) R_n$$

- Aliasing
- Redundancy

Fourier Transform





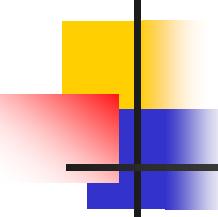
Fourier Transform

- Uncertainty
 - Bandwidth

$$\frac{N-1}{2} \cdot \frac{1}{N\Delta t} \approx \frac{1}{2\Delta t}$$

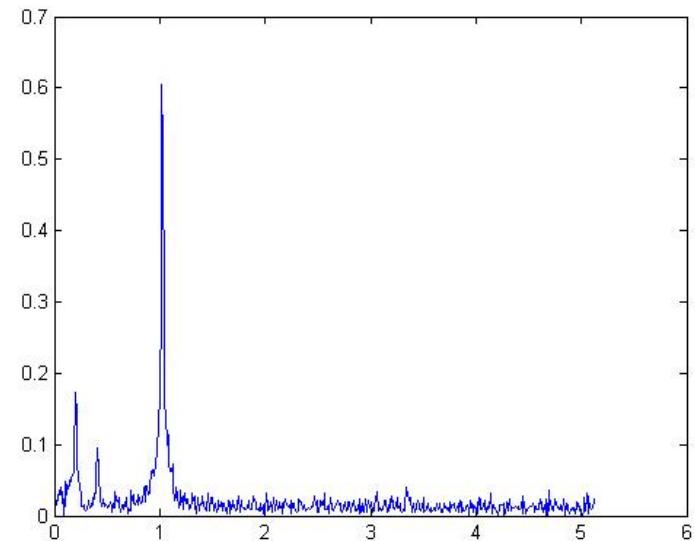
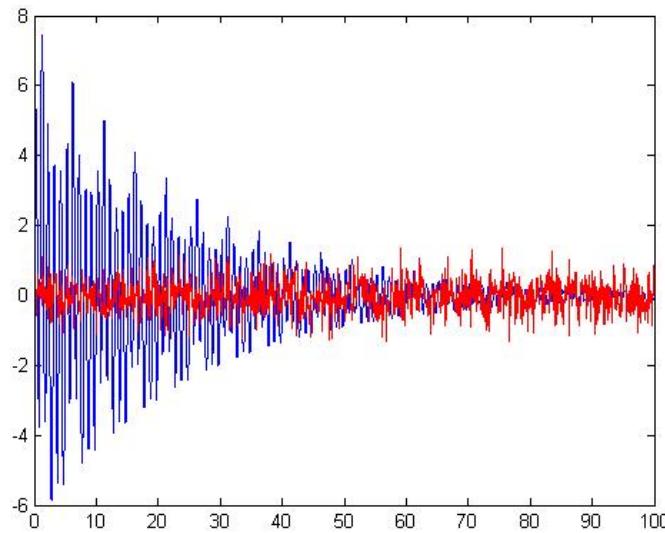
- Time/Frequency resolution

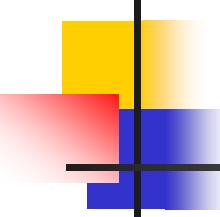
$$\Delta t \Delta f = \frac{1}{N}$$



Fourier Transform

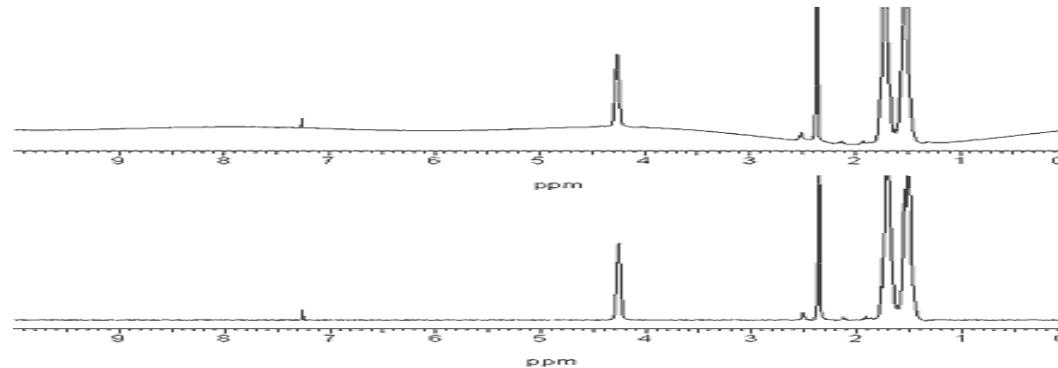
- NMR-signals:
 - exponential decay
 - noise





Data refinement

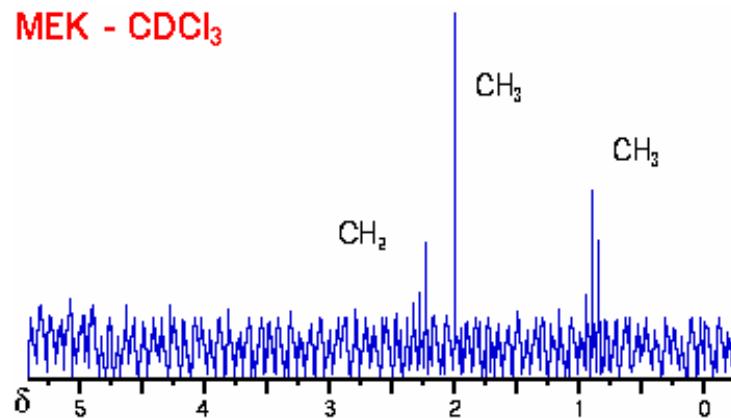
- Baseline correction



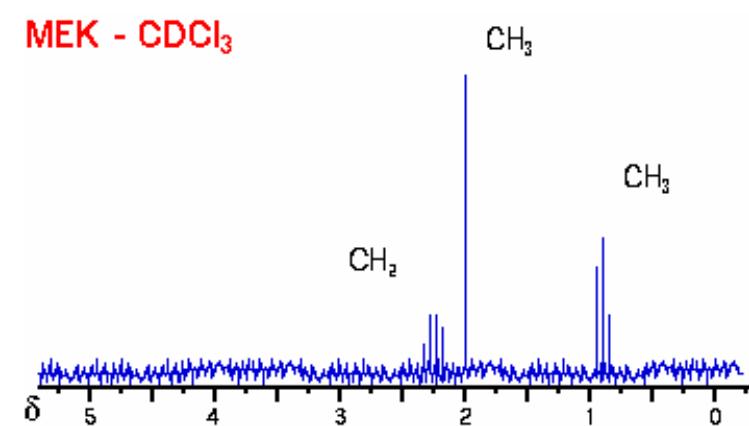
- First point extrapolation
- Adopization (weighting)
- Zero filling

Averaging

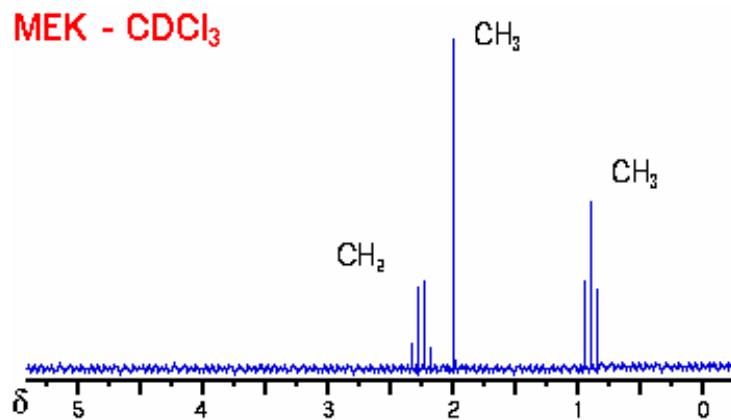
MEK - CDCl_3



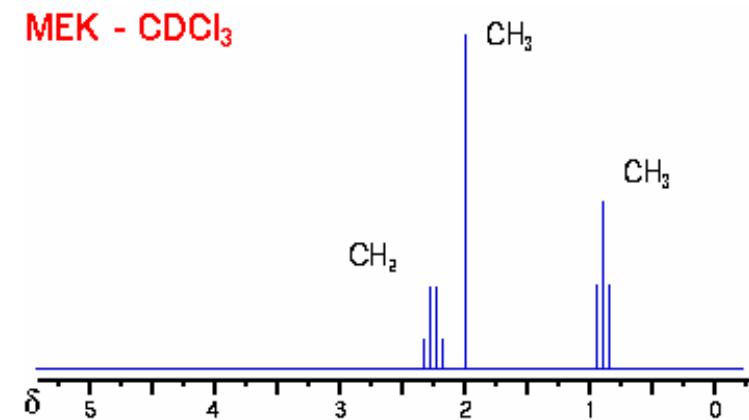
MEK - CDCl_3



MEK - CDCl_3



MEK - CDCl_3



THANK YOU FOR YOUR ATTENTION!

